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2 3	Monitoring Therapeutic Response to Anti-FAP CAR T Cells using [¹⁸ F]AIF-FAPI-74
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5 6 7 8	Iris K. Lee ^{1,2} , Estela Noguera-Ortega ³ , Zebin Xiao ⁴ , Leslie Todd ⁴ , John Scholler ⁵ , Decheng Song ⁵ , Maria Liousia ³ , Katheryn Lohith ² , Kexiang Xu ² , Kimberly J. Edwards ² , Michael D. Farwell ² , Carl H. June ⁵ , Steven M. Albelda ^{3,5} , Ellen Puré ⁴ , Mark A. Sellmyer ^{2,6} *
9	1. Department of Bioengineering, University of Pennsylvania, Philadelphia, PA, USA. 2. Department of
10	Radiology, Perelman School of Medicine, University of Pennsylvania, Philadelphia, PA, USA. 3.
11	Department of Medicine, Perelman School of Medicine, University of Pennsylvania, Philadelphia, PA
12	USA. 4. Department of Biomedical Sciences, School of Veterinary Medicine, University of Pennsylvania,
13	Philadelphia, PA, USA, 5. Center for Cellular Immunotherapies, Perelman School of Medicine, University
14	of Pennsylvania, Philadelphia, PA, USA. 6. The Deparment of Biochemistry and Biophysics, Perelman
15	School of Medicine, University of Pennsylvania, Philadelphia, PA, USA.
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17	
18 19	* Correspondence should be addressed to:
20	M.A.S. (mark.sellmyer@pennmedicine.upenn.edu) https://orcid.org/0000-0002-1407-1905
20	https://orcid.org/0000-0002-1407-1905
22	Department of Radiology
23	Perelman School of Medicine at the University of Pennsylvania
24	813A Stellar-Chance Labs
25	422 Curie Boulevard
26	Philadelphia, PA 19104-6059
27	Phone: 215-573-3212
28	
29	Running Title: Monitoring response to CAR T cell therapy using PET imaging
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31	Keywords: Cellular therapy, FAP, biomarkers, molecular imaging, PET
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33	Synopsis: A PET imaging approach targeting fibroblast activation protein (FAP) expressed on activated
34	fibroblasts of the tumor stroma has the potential to predict and monitor therapeutic response to FAP-
35	targeted CAR T cell therapy
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39 Translational Relevance

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41 Precision medicine is an emerging theme in modern cancer therapy, with the goal of tailoring treatments

42 based on the presence or absence of certain biomarkers in the tumor. Approaches to targeted therapies

43 have diversified, including genetically engineered cell therapies like chimeric antigen receptor (CAR) T

44 cells. However, current tools to predict and monitor therapeutic responses to these dynamic, "living 45 drugs" are limited. Here we show that a positron emission tomography (PET) radiotracer [¹⁸F]AIF-FAPI-74

46 targeted to fibroblast activation protein (FAP), a pan-tumor marker expressed by activated fibroblasts in

47 the tumor microenvironment, is able to image FAP expression in pre-clinical tumor models with high

48 sensitivity. Coupled with FAP-targeted CAR T cells, [¹⁸F]AIF-FAPI-74 PET imaging demonstrated successful

49 clearance of FAP⁺ cells following therapy, with a high correlation of PET signal to FAP signal quantified

50 using immunohistochemistry. Our study highlights the potential role of $[^{18}F]AIF$ -FAPI-74 as a predictive

51 and pharmacodynamic imaging biomarker for FAP-targeted therapies in assessing the target

52 biodistribution and informing patient selection, as well as in monitoring response to therapy.

53 Abstract

54

Purpose: Despite the success of chimeric antigen receptor (CAR) T cell therapy against hematological malignancies, successful targeting of solid tumors with CAR T cells has been limited by a lack of durable responses and reports of toxicities. Our understanding of the limited therapeutic efficacy in solid tumors could be improved with quantitative tools that allow characterization of CAR T-targeted antigens in

59 tumors and accurate monitoring of response.

60

61 **Design**: We used a radiolabeled fibroblast activation protein (FAP) inhibitor (FAPI) [¹⁸F]AIF-FAPI-74 probe

62 to complement ongoing efforts to develop and optimize FAP CAR T cells. The selectivity of the radiotracer

63 for FAP was characterized *in vitro* and its ability to monitor changes in FAP expression was evaluated using

- 64 rodent models of lung cancer.
- 65

66 **Results**: $[^{18}F]$ AIF-FAPI-74 showed selective retention in FAP⁺ cells *in vitro*, with effective blocking of the 67 uptake in presence of unlabeled FAPI. *In vivo*, $[^{18}F]$ AIF-FAPI-74 was able to detect FAP expression on both

68 tumor cells as well as FAP⁺ stromal cells in the tumor microenvironment with a high target-to-background

- 69 ratio. We further demonstrated the utility of the tracer to monitor changes in FAP expression following
- 70 FAP CAR T cell therapy, and the PET imaging findings showed a robust correlation with *ex vivo* analyses.
- 71

72 **Conclusion**: This non-invasive imaging approach to interrogate the tumor microenvironment represents

an innovative pairing of a diagnostic PET probe with solid tumor CAR T cell therapy and has the potential

to serve as a predictive and pharmacodynamic response biomarker for FAP as well as other stromal cell-

75 targeted therapies.

76 Introduction

77

78 Recent breakthroughs in chimeric antigen receptor (CAR) T cell therapy have positively transformed the 79 management of many hematological malignancies (1). With such success, adoptive cell therapy is being 80 explored for the treatment of solid tumors (2). The effort to extend the benefits of CAR T therapy to other 81 cancers, however, is challenged by a lack of therapeutic efficacy and reports of severe toxicities. Robust 82 biomarkers that can help identify patients likely to benefit from the therapy and accurately assess 83 treatment response are needed to improve the safety of the therapy for patients. This problem is 84 especially true in the context of CAR T cell treatment for solid tumors given the lack of uniformly expressed 85 tumor-specific markers across different solid tumor types, which increases concern for on-target/off-86 tumor toxicities (3). Identification of biomarkers that can provide insights on the likelihood, as well as 87 presence or absence of a therapeutic response, will help maximize the therapeutic potential of these 88 "living drugs" and help inform patient management early in the treatment course.

89

90 The microenvironment surrounding tumor cells is a complex and dynamic system integral to solid tumor 91 pathogenesis (4). Thus, the tumor microenvironment (TME) and supporting cells in the tumor stroma, 92 which can be present across many different tumor types, make the TME a promising target to potentiate 93 treatments like immunotherapies (5). Specifically, fibroblast activation protein (FAP), a cell surface serine 94 protease that is highly expressed on cancer-associated fibroblasts (CAFs) in over 90% of epithelial cancers 95 (6,7), has emerged as a pan-tumor target (8). Given increasing evidence that FAP and FAP⁺ cells play a vital 96 role in the remodeling of the tumor microenvironment and tumor progression, many FAP-targeted 97 therapies - such as vaccines (9) and immunotherapies (10) - are in development. In concert with 98 therapeutic developments targeting FAP, imaging probes which can quantitatively measure FAP 99 expression have shown remarkable results. A recent retrospective analysis of patients imaged with 100 Gallium-labeled FAP inhibitor ([68Ga]-FAPI-04) showed significant tracer uptake in a variety of primary, 101 metastatic, and recurring solid tumor entities (11), highlighting that such "universal" overexpression of 102 FAP across different solid tumors not only make it a promising therapeutic target, but also a useful 103 biomarker to assess for diagnosis and staging of different solid tumors.

104

105 Here, we investigate the use of [¹⁸F]AIF-FAPI-74 PET pre-clinical imaging and its potential role in predicting 106 and monitoring response to FAP CAR T cell therapy. FAP-targeted CAR T cells have demonstrated a 107 significant anti-tumor effect in several pre-clinical solid tumor models including pancreatic cancers and 108 mesothelioma (12-14). In this work, we characterize the *in vitro* and *in vivo* uptake of [¹⁸F]AIF-FAPI-74 by 109 FAP-expressing cells. We also demonstrate the utility of the tracer for monitoring therapeutic response 110 following administration of a novel FAP (4G5) CAR T cell therapy in a pre-clinical lung carcinoma model 111 that induces the formation of native mouse stroma. Using PET to help identify patients who are most likely 112 to respond to the therapy based on the level of FAP expression in the tumor and monitor their response 113 to the FAP-targeted CAR T cells could be key for clinical translation and integration of the therapy for 114 patient management. Monitoring FAP expression over time could provide a direct way to assess the 115 efficacy of FAP CAR T cell therapy by measuring how the target FAP-expressing cells are depleted in 116 response, which is in contrast to traditional approaches that focus on tracking changes in tumor size 117 during treatment, and could provide early insight into treatment success or failure. 118

- 119 Methods
- 120

121 Chemical Synthesis

122 The FAPI-74 precursor was synthesized by ABX advanced biochemical compounds gmbH (Radeberg,

123 Germany). The manufacturing process of [¹⁸F]AIF-FAPI-74 final drug product (Figure 1A) was adapted from

the manual process developed by Giesel *et al.* (15) and was carried out by SOFIE Biosciences, Inc. (Totowa, New Jersey, USA) on a Trasis miniAllinOne radiosynthesizer. Specific activity ranged from 2.43×10^{4} -9.37x10⁴ mCi/mg or 661.67-2550.14 GBq/µmol. Methods on chelator conjugation, radiolabeling, and quality control of the final, radiolabeled full-length 4G5 FAP antibody are described in the supplemental information under "DFO-Conjugation of Antibodies" and "Radiolabeling of Antibodies with Zirconium-89 (⁸⁹Zr)".

130

131 Cell Lines

Human mesothelioma cell line I45 wild type (WT) was originally derived from a sarcomatoid pleural mesothelioma and provided by Dr. Joseph Testa (Fox Chase Cancer Center, Philadelphia, PA). I45 cells were transduced with a lentivirus encoding human FAP and then flow-sorted to enrich for I45 huFAP cells. The human lung adenocarcinoma cell line A549 was purchased from the ATCC (ATCC CCL-185TM). Cells were maintained in RPMI 1640 supplemented with 10% fetal bovine serum (FBS), 100 U/mL penicillin, and 100 µg/mL streptomycin sulfate, and cells were detached using Versene to prevent cleavage of FAP from the cell surface. All reagents were purchased from Therme-Ficher Scientific

138 the cell surface. All reagents were purchased from ThermoFisher Scientific.

139

140 In Vitro Cell Uptake Study

141 3x10⁶ I45 WT and I45 huFAP cells were incubated with 6x10⁶ counts per minute (cpm) (which corresponds 142 to ~90-100µCi or ~3.3-3.7MBg) of [¹⁸F]AIF-FAPI-74 for 60 minutes in the presence or absence of unlabeled 143 10µM FAPI-74 in media. Following incubation, cells were centrifuged at 1200 rpm and washed 3 times 144 with cold PBS (21-031-CM, Corning). After the third wash, the cell pellet was resuspended in 600µL of PBS 145 and split into 3 technical replicates of 200µL. Radiotracer uptake was quantified on a gamma counter 146 (PerkinElmer) and analyzed by dividing counts by the counts of incubated dose of [¹⁸F]AIF-FAPI-74 147 (injected dose; ID). The final uptake was reported as %ID normalized per 10⁶ cells (%ID/10⁶ cells). In vitro 148 cell uptake studies with the full-length 4G5 antibody are described in the supplemental information under 149 "In Vitro Cell Uptake Study with [89Zr]DFO-4G5."

150

151 Generation of 4G5 Hybridoma

152 Full-length canine FAP cDNA was cloned by PCR from total RNA extract of canine osteosarcoma cells, SK 153 KOSA. The PCR product was sequenced and cloned into pLenti/v5-D-TOPO which was used to generate 154 virus and transduce Balb/C 3T3 cells. FAP-null mice were immunized and boosted four times 155 intraperitoneally with the 3T3 cells expressing caFAP. Three days after the final boost, splenocytes were 156 harvested and fused to myeloma cells. Hybridoma supernatants were screened by flow cytometry for 157 mAbs that reacted specifically with MC KOSA.caFAP cells but not the parental MC KOSA cells which are 158 negative for FAP. Clone 4G5 was further screened against MC KOSA canine osteosarcoma cells, mouse 159 dermal fibroblasts, and human foreskin fibroblasts expressing canine, mouse, and human FAP, 160 respectively, and showed species cross-reactivity (Figure S1). ThermoFisher Rapid ELISA Mouse mAB 161 Isotyping kit (#37503) was used to determine IgG1k isotype.

162

163 Generation of Anti-FAP CAR Construct

164 Total RNA isolated from 4G5 hybridoma cell line was reverse transcribed (Takara, Cat# RR057A) into 165 cDNAs and PCR amplified using a library of mouse variable chain primers (Progen Cat# F2010) to identify 166 hybridoma sequence. Additionally, 5' RACE was used to validate 5' most sequences (Invitrogen, 167 Cat#18374058), these amplified bands were TOPO cloned and sequenced. The procedures were repeated 168 to confirm the integrity of identified sequences. All isolated and sequence-verified ORFs of variable chains 169 were synthesized and used in heavy and light chain combinations to obtain desired performing scFV in 170 CAR format. For this study, a CAR construct containing the V_L and V_H sequences (L2HG) followed by CD8 α

171 hinge, CD8α transmembrane domain, and two human intracellular signaling domains (ICD) derived from

- 172 4-1BB and CD3ζ was synthesized and cloned into pTRPE lentiviral plasmid. This CAR targets both human
- 173 and murine FAP-expressing cells. A T2A-mCherry gene was cloned downstream of the L2HG FAP CAR
- 174 domain for assessment of transduction and flow-based sorting of CAR⁺ T cells (Figure 4A).
- 175

176 Generation of CAR T Cells

- Primary human T cells collected from healthy volunteers were obtained from the Human Immunology
 Core at the University of Pennsylvania. All human specimens were collected under University Institutional
- 179 Review Board-approved protocols following informed consent from the volunteers. Bulk T cells
- 180 (containing both CD4⁺ and CD8⁺) were activated and expanded by incubating with anti-CD3/anti-CD28
- 181 antibody-coated magnetic beads (Dynabeads, Thermo Fisher Scientific) at a ratio of 3:1 beads to T cells.
- 182 Following 16 hours of incubation with the beads, pTRPE FAP CAR-T2A-mCherry lentivirus (prepared as
- 183 previously described (16)) was added to the T cells at an MOI of 5. The T cells were expanded for 10 days
- 184 before characterization and cell sorting.
- 185 186 Elow Cute

186 Flow Cytometry

- FAP CAR-T2A-mCherry T cells were pelleted, resuspended in 2% BSA in PBS (Invitrogen), and incubated
 with Alexa Fluor[®] 647 AffiniPure F(ab'2) fragment goat anti-mouse IgG (Jackson ImmunoResearch
 Laboratories) for 30 minutes at room temperature. Stained cells were analyzed on an LSR II flow cytometer
- (BD Biosciences) for mCherry and CAR expression, and flow data were analyzed using FlowJo software.
- 191

192 Cytotoxicity and Cytokine Release Assay

- 193 1x10⁴ of I45 WT and I45 huFAP target cells were seeded into 96-well plates. The following day, either non-
- 194 transduced (NTD) but activated control T cells or effector FAP CAR-T2A-mCherry T cells were added to
- the target cells at a range of effector-to-target (E:T) ratios from 2.5:1 to 20:1. Following an overnight co-
- 196 incubation of T cells and target cells, supernatants were collected to quantify IFN γ and TNF α release by
- 197 ELISA (Abcam), and target cell viability was assessed using CellTiter 96[®] Aqueous Non-Radioactive Cell
- 198 Proliferation Assay (MTS) (Promega).

199

200 I45 Mesothelioma Model

- 201 6- to 8-week-old female immunodeficient NOD-SCID-*Il2rq^{-/-}* (NSG) mice were obtained from Penn Stem 202 Cell & Xenograft Core and subcutaneously xenografted with 1x10⁶ I45 WT cancer cells on the left flank 203 and 1x10⁶ I45 huFAP cancer cells on the right flank in 100µL of PBS. Following 2 weeks of tumor growth, 204 when tumors reached ~100-150mm³, animals were administered ~200-250µCi [¹⁸F]AIF-FAPI-74 via tail 205 vein and then anesthetized under 2% isoflurane for PET/CT imaging on a small animal PET/CT (Molecubes) 206 1 hour post-radiotracer administration. For image analysis, 3-dimensional (3D) elliptical regions of interest 207 (ROIs) were drawn around the tumor and muscle (background organ) using the CT images as a reference, 208 and the ROIs were copied to PET. The maximum and mean counts from each ROI were quantified using 209 MIM (MIM Software). The ratio of tracer uptake between tumor and muscle (tumor-to-muscle ratio) was 210 calculated by dividing SUV_{max} of tumor by SUV_{max} of muscle, or dividing SUV_{mean} of tumor by SUV_{mean} of 211 muscle. PET image scale bar is represented in unit of Scaled Threshold of SUV_{body weight} (SUV_{bw}) and CT 212 image scale bar is Houndsfield Unit (HU). PET studies with [89Zr]DFO-4G5 are described in the supplemental information under "[89Zr]DFO-4G5 Small Animal PET Imaging". 213
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215 A549 Lung Adenocarcinoma Model

- 216 6- to 8-week-old female immunodeficient NSG mice were subcutaneously xenografted with 1x10⁶ A549
- 217 $\,$ cancer cells on the right flank in 100 μL of PBS. Following 3 weeks of tumor growth, when the tumors
- 218 reached ~100-150mm³, [¹⁸F]AIF-FAPI-74 PET/CT imaging was performed and analyzed as described above.
- 219 For the clearance experiment with FAP CAR T cells, all mice were injected intravenously (i.v.) with either

5x10⁶ CAR⁺ FAP CAR-T2A-mCherry T cells or non-transduced (NTD) control T cells the day after baseline
 [¹⁸F]AIF-FAPI-74 PET/CT imaging was performed. A follow-up scan was performed 14 days post-T cell
 injection.

223

224 Ex Vivo Biodistribution and Tissue Analysis

225 Mice were sacrificed following terminal [¹⁸F]AIF-FAPI-74 PET/CT imaging. Various tissues were harvested 226 for ex vivo biodistribution analysis and the level of uptake in each organ was measured using a gamma 227 counter (PerkinElmer) and quantified as %ID per gram of organ (%ID/g). Tumor tissues were digested in a 228 solution of BD Horizon™ Dri Tumor & Tissue Dissociation Reagent (BD Biosciences) for 30 minutes at 37°C. 229 Digested tumors were filtered through 70µm nylon mesh cell strainers (Fisher Scientific), and red blood 230 cells were lysed as needed (Pharm Lyse, BD Biosciences). Single-cell suspensions (1×10⁶ cells) were stained 231 with PE-Dazzle 594-conjugated anti-human CD45 antibody (344744, Biolegend). Ex vivo biodistribution 232 analysis of [⁸⁹Zr]DFO-4G5 is described in the supplemental information under "Ex Vivo Biodistribution 233 Analysis of "[⁸⁹Zr]DFO-4G5 in Healthy (Non-Tumor Bearing) Animals".

234

235 Immunohistochemistry

236 Samples were frozen in OCT-embedding media on dry ice. 5µm sections were generated using a Cryostat 237 (Leica CM 1950), mounted on glass slides (12-550-15, Fisher Scientific), and dried. Sections were washed 238 with PBS for 5 minutes, incubated with blocking buffer containing 3% BSA (BSA-50, Rocklandand) and 0.3% 239 Triton X-100 (10789704001, Roche) in PBS (21-031-CM, Corning) for 1 hour, and then stained with primary 240 antibodies in blocking buffer overnight at 4°C. The following primary antibodies were used: rabbit 241 monoclonal anti-fibroblast activation protein alpha (FAP- α ; ab207178, Abcam), goat polyclonal anti-242 platelet-derived growth factor receptor alpha (PDGFRa; AF1062, R&D system), and FITC-conjugated 243 mouse anti-mouse/human α -smooth muscle actin (F3777, Millipore Sigma). Following staining with 244 primary antibodies, slides were blocked again for 1 hour and then incubated with secondary antibodies in 245 the blocking buffer for 1 hour. All secondary antibodies (Alexa 555 Donkey anti-rabbit IgG (A32794) and 246 DyLight 650 Donkey anti-goat IgG (84545)) were purchased from Invitrogen. Slides were washed 3 times 247 and mounted in ProLong[™] Diamond Antifade Mountant with DAPI (P36971, ThermoFisher). Low-248 magnification and high-magnification photos were taken using a Nikon NIS-Elements microscope and all 249 images were processed using ImageJ.

250

251 Statistical Analyses

All the statistical data analysis was performed on Prism 9 (GraphPad). An unpaired, two-tailed student ttest was used to determine statistical significance between two groups. For comparisons of more than two groups, one-way or two-way ANOVA was performed with appropriate *post hoc* testing. A p-value of

- 255 <0.05 was considered to be statistically significant. All data points are presented as mean \pm SD. 256
- 257 Results
- 258

259 An ImmunoPET approach demonstrates limited dynamic range in detecting FAP *in vivo*

260 To identify the in vivo antigen target of FAP-directed CAR T cells, and thereby serve as a predictive 261 biomarker of FAP CAR T cell therapy, one approach would be to use an immunoPET agent. In this 262 approach, the antibody-derived radiotracer shares the identical clonal origin and the single-chain variable 263 fragment (scFv) that will bind the same epitopes as the FAP CAR T cells. The Puré lab developed a mouse 264 IgG1k monoclonal antibody, 4G5, against canine FAP that cross-reacts with human and mouse FAP (Figure 265 s1). A CAR was engineered based on the 4G5 monoclonal antibody and cloned into a lentiviral vector 266 encoding 4G5 anti-FAP scFv (4G5)-CD8 hinge-4-1BB-CD3z. In order to test whether we can detect FAP 267 expression using the 4G5 antibody that is parent to the FAP CAR T cell therapy in development, we

radiolabeled the full-length 4G5 FAP antibody with ⁸⁹Zr to develop a [⁸⁹Zr]DFO-4G5 immunoPET probe. 268 269 Successful conjugation of 4G5 to chelator deferoxamine (DFO) – with a degree of labeling (DOL) of 2.6 270 DFO molecules per antibody – was confirmed by MALDI-TOF (Figure S3A). The radiochemical yield of ⁸⁹Zr 271 radiolabeling ranged from 70-82% with a specific activity of 6.5-9.3mCi/mg and the free ⁸⁹Zr in the final 272 product, as assessed by radio TLC, was minimal (Figure S3B). Methods of DFO-conjugation, radiolabeling 273 of the antibody, and subsequent downstream assays performed with [89Zr]DFO-4G5 are described in the 274 supplemental information. To evaluate the ability of [89Zr]DFO-4G5 to selectively bind to FAP, an in vitro 275 cell uptake experiment was performed with: I45 WT (which do not express FAP) and I45 cells transduced 276 to express human FAP (I45 huFAP) (Figure S2). The uptake study showed a 54-fold higher tracer uptake in 277 145 huFAP cells compared to 145 WT, demonstrating a high specificity of the [89Zr]DFO-4G5 immunoPET 278 probe for FAP (Figure S3C). Co-incubation of the radiotracer with excess unlabeled 4G5 antibody 279 successfully competed with and reduced the uptake of the radiotracer by I45 huFAP, further 280 demonstrating the specificity of the radiotracer uptake via FAP binding.

281

282 Given the high specificity demonstrated in the uptake study, the [89Zr]DFO-4G5 radiotracer was next 283 tested for its ability to detect FAP expression in two different tumor xenograft models: 1) I45 284 mesothelioma (non-stromagenic) and 2) A549 lung adenocarcinoma model where the tumor cells do not 285 express FAP but drive the generation of FAP⁺ stromal cells in the tumor microenvironment in vivo (13). 286 For the I45 model, the I45 WT and I45 huFAP tumor cells were xenografted on opposite flanks of 287 immunodeficient NSG mice. Following 2 weeks of tumor growth, [89Zr]DFO-4G5 radiotracer was 288 administered via tail vein and PET/CT images were acquired 72 hours post-radiotracer administration. In 289 this I45 model, [⁸⁹Zr]DFO-4G5 PET/CT uptake was 3-fold higher in the I45 huFAP tumor compared to the 290 145 WT (Figure S3D). Ex vivo anti-FAP IHC and autoradiography on tumor sections further supported the 291 imaging findings (Figure S4B). For the A549 model, the cells were also xenografted on the flank of NSG 292 mice and grown for 3 weeks. The A549 tumor showed approximately 8 to 9-fold increased radiotracer 293 uptake relative to the muscle (Figure S3E), and this was further supported in the ex vivo biodistribution 294 analysis (Figure S4A, right panel).

295

296 Despite the promising data showing a robust accumulation of the tracer in FAP-expressing tumors, a few 297 limitations of this approach became apparent in the validation process. Both PET imaging and ex vivo 298 biodistribution analysis showed evidence of tracer uptake in non-target expressing I45 WT tumor that was 299 around 5-fold higher than the background, which demonstrates potential non-specific accumulation of 300 antibody-based probe in areas of leaky tumor vasculature (Figure S3D and Figure S4A, left panel). Lastly, 301 as a full-length IgG radiotracer, [89Zr]DFO-4G5 exhibited slow accumulation and clearance kinetics (Figure 302 S4C), and PET imaging had to be performed 3 days following tracer injection to ensure optimal target-to-303 background ratio. While this was feasible to accommodate for pre-clinical imaging studies, same-day 304 imaging would be ideal for a future clinical workflow. As small molecule-based imaging probes are rapidly 305 cleared from blood due to their relatively small size and will thereby help improve the target-to-306 background ratios, we next evaluated the use of a known radiolabeled small molecule inhibitor of FAP 307 (FAPI), [¹⁸F]AIF-FAPI-74, as an alternative PET radiotracer to monitor FAP expression and thereby 308 complement FAP-targeted therapies.

309

310 Small molecule-based [¹⁸F]AIF-FAPI-74 radiotracer exhibits high specificity for FAP

311 The specificity of [¹⁸F]AIF-FAPI-74 tracer (Figure 1A) for FAP was tested by performing an *in vitro* cell

312 uptake experiment with I45 cells. The uptake study showed significantly higher tracer uptake of over 100-

fold in the I45 huFAP cells compared to the I45 WT. This uptake was effectively competed by the addition

- of an excess of unlabeled FAPI, demonstrating rapid and highly specific binding of [¹⁸F]AIF-FAPI-74 tracer
- 315 to FAP *in vitro* (Figure 1B).

316

317 [¹⁸F]AIF-FAPI-74 imaging of FAP in xenograft tumor models demonstrates enhanced sensitivity and 318 dynamic range

319 To evaluate the ability of the [¹⁸F]AIF-FAPI-74 radiotracer to detect FAP expression in animals, we tested 320 the FAPI tracer in both the I45 mesothelioma and A549 lung adenocarcinoma model used for the initial 321 validation of the [⁸⁹Zr]DFO-4G5 radiotracer. In the I45 model, [¹⁸F]AIF-FAPI-74 uptake was higher by 7.5-322 fold in the I45 huFAP tumor compared to the I45 WT (Figure 2A and 2B). This degree of uptake was more 323 than 2-fold higher than what was observed with [89Zr]DFO-4G5 (Figure S3D). Ex vivo biodistribution 324 analysis further supported and validated the PET imaging findings, with 12 and 15-fold increased tracer 325 retention in the I45 huFAP tumor relative to the I45 WT tumor and background organs, respectively 326 (Figure 2C). To validate that the increased PET signal in the I45 huFAP tumor was in fact due to its FAP 327 expression, we performed anti-FAP IHC and showed selective expression of FAP in the I45 huFAP tumor 328 (Figure 2D). Probing for α -smooth muscle actin-positive (α SMA⁺) myofibroblasts and platelet-derived 329 growth factor receptor α -positive (PDGFR α^+) cells (which represent subpopulations of the heterogenous 330 CAFs found in the tumor microenvironment (17)), we did not detect significant numbers of CAFs in the 331 non-stromagenic I45 WT or I45 huFAP tumors as expected, indicating that the PET signal is mainly 332 attributable to uptake by the I45 cells engineered to express FAP.

333

334 In the A549 model, animals xenografted with the tumor showed approximately 4 to 6-fold increased 335 [¹⁸F]AIF-FAPI-74 uptake in the A549 tumor relative to the muscle (Figure 3A and 3B). As A549 cells do not 336 express FAP, the PET signal in this model is attributable to FAP⁺ stromal cells in the tumor 337 microenvironment. We were able to clearly identify fibroblasts in this stromagenic tumor with IHC (Figure 338 3C). IHC images of the A549 showed a variable pattern of FAP expression related to fibroblast invasion 339 and recruitment to the stroma, compared to the I45 model which exhibited a more homogenous 340 population of FAP⁺ cells given its expression by the tumor cells themselves. An imaging study with FAP 341 knockout (KO) NSG mice bearing A549 tumors showed an absence of tracer uptake in the area of the 342 tumor (Figure S5), demonstrating that our [¹⁸F]AIF-FAPI-74 tracer is specific for FAP and detects host 343 stromal cells.

344 345 [¹⁸F]AIF-FAPI-74 PET/CT imaging has utility in monitoring therapeutic response following FAP CAR T cell 346 therapy

Given that [¹⁸F]AIF-FAPI-74 can provide semi-quantitative index of FAP expression in the tumor microenvironment- the target of FAP-directed therapies – it has the potential to not only serve as a predictive biomarker that can be used to stratify patients who are likely to respond to therapy but also as a downstream measure of therapeutic efficacy (i.e. how effective FAP-targeted therapies are at ablating the target FAP⁺ cells). In order to test this premise, we evaluated whether [¹⁸F]AIF-FAPI-74 tracer can detect clearance of FAP⁺ cells in the more challenging, biologically relevant A549 tumor model following FAP CAR T cell treatment.

354

For these studies, we utilized a new FAP CAR construct based on the scFv of the 4G5 antibody which also expressed mCherry as a marker gene (**Figure 4A**). We first demonstrated good expression levels of both the CAR and mCherry in transduced human T cells (**Figure 4B**). We next confirmed their antigendependent ability to effectively kill I45 huFAP cells and spare non-FAP expressing I45 WT cells in an *in vitro* cytotoxicity study (**Figure 4C**). Supernatants collected from the killing assay confirmed the release of IFNy when the effector cells were co-incubated with FAP⁺ target cells, indicating FAP-specific CAR T cell activation (**Figure 4D**).

362

363 NSG mice bearing 100-150mm³ A549 tumors were injected with either 5x10⁶ FAP CAR⁺ T cells or non-364 transduced (NTD) control T cells following a baseline [¹⁸F]AIF-FAPI-74 scan. Tumor volumes were 365 measured every 3-4 days, and a follow-up scan was performed on Day 14 post-T cell injection (Figure 5A). 366 At this 14-day time point, mice treated with FAP CAR T cells had significantly smaller tumors (p<0.01) 367 relative to the NTD control T cell-treated group, highlighting the therapeutic efficacy of the FAP CAR T cell 368 therapy (Figure 5B).

369

In the follow-up [¹⁸F]AIF-FAPI-74 scan, there was no detectable tracer uptake in the area of tumor in mice that received FAP CAR T cell therapy while the NTD control T cell-treated group had a significant accumulation of tracer in the tumor region (**Figure 5C**). Quantification of PET images showed that the tumor-to-muscle ratio decreased for FAP CAR T cell-treated group by 2 to 3-fold relative to the baseline scan, highlighting that the [¹⁸F]AIF-FAPI-74 is a sensitive tool that allows imaging of FAP clearance from the tumor following a FAP-targeted therapy (**Figure 5D**). Furthermore, we observed a robust correlation between the caliper measurements and tumor volume assessed by CT (**Figure S6**).

377

378 To further validate the PET imaging findings, ex vivo analyses were performed after the terminal follow-379 up [¹⁸F]AIF-FAPI-74 PET/CT scan. We observed a marked 3.5-fold higher retention of the tracer in the 380 harvested tumors treated with NTD T cells relative to the FAP CAR T cell-treated tumors (Figure 6A). While 381 uptake in normal background tissues (blood, eye, spleen, muscle) was very low and comparable across 382 the control and FAP CAR-treated groups, there was a statistically significant difference in bone and 383 marrow uptake between the two groups. Flow analysis of cell population in the A549 tumor showed a 384 higher percentage of total CD45⁺ T cells in the CAR T-treated group relative to the NTD T cell-treated 385 group, which indicated specific CAR T cell infiltration in the tumors (Figure 6B). To further validate PET 386 imaging findings, we again performed correlative anti-FAP, anti- α SMA, and anti-PDGFR α^+ IHC on the FAP 387 CAR T-treated and NTD T cell-treated A549 tumors. Treatment with FAP CAR T cells abolished all 388 subpopulations of CAFs, supporting that the lack of PET imaging signal in the tumor area is due to the 389 successful depletion of FAP⁺ cells (Figure 6C). Disruption of all of the CAFs is expected in the FAP CAR T 390 cell-treated group given that FAP⁺ cells often co-express SMA and PDGFRa (17). Moreover, FAP⁺ cells have 391 shown to be critical to the recruitment and/or differentiation of SMA⁺ myofibroblasts, and therefore 392 depletion of FAP⁺ cells will also disrupt the network of SMA⁺ myofibroblasts as demonstrated in the IHC 393 (13). 394

- 395 Discussion
- 396

397 The ability to monitor the biological target of a living drug such as CAR T cells is an important strategy 398 where molecular imaging can support improvement and development of next-generation therapies (18). 399 Here, we found that the inherent characteristics of small molecule-based radiotracers, such as the rapid 400 clearance from background organs, allowed for high contrast imaging, and have advantages to 401 characterize FAP expression compared to antibody-based immunoPET that requires conjugation to 402 longer-lived isotopes. We demonstrated that [¹⁸F]AIF-FAPI-74 extends beyond its role as a companion 403 diagnostic (in predicting response) and can also serve as a "pharmacodynamic" biomarker to assess the 404 downstream efficacy of a therapy. Thus, this approach has the potential to aid in both patient selection 405 and in monitoring response to FAP-targeted therapies, including living drugs such as FAP CAR T cells as 406 demonstrated here. Although similar tools, namely [89Zr]-Atezolizumab (19) and [18F]-FluorThanatrace 407 (20), have been developed to help predict patient benefit from cancer therapies such as PD-1/PD-L1 408 checkpoint blockade therapy and PARP inhibitors, respectively, this work builds on these prior studies and 409 demonstrate how a companion diagnostic tool can also be applied for a living drug where therapeutic 410 production costs are significant. FAP-specific antibody-drug conjugates (ADCs) (21), tumor vaccines

411 against FAP (9), and radionuclide therapy with [¹⁷⁷Lu]FAPI-46 (22) are other FAP-targeting strategies that 412 will use and benefit from [¹⁸F]AIF-FAPI-74 imaging in a theranostic approach.

413

414 FAP-targeted nuclear imaging has been previously attempted with FAP antibodies (23,24) and boronic 415 acid-based FAP inhibitors (25). However, given the extended half-life of these agents in the blood and 416 poor target-to-blood ratio, quinoline-based small molecule FAPI tracers that offer high specificity and 417 rapid blood clearance have ascended (26). Furthermore, FAPI tracers have already demonstrated 418 potential as a diagnostic tool in different clinical settings beyond oncology, including in cardiovascular and 419 autoimmune-mediated diseases (11,27-29). Our choice of the [¹⁸F]AIF-FAPI-74 was informed by the 420 extensive work of the Heidelberg group and medicinal chemistry optimization of FAPI compounds, several 421 of which are near clinical translation (15). Similar to the observations in the field, while our 4G5 antibody-422 based immunoPET approach allowed us to visualize the antigenic target of FAP-directed CAR T cells given 423 the shared scFv domains between the companion diagnostic and the therapeutic, the slow accumulation 424 and clearance kinetics of the full-length antibody did not provide as high of sensitivity compared to the 425 small molecule FAPI approach (Figure S3D-S3E). Given that the tracer and the therapeutic share the same 426 scFv domain, there is also a potential concern that the long half-life of the tracer may competitively inhibit 427 CAR T antigen on the tumor and prevent the CAR T cells from eliciting cytotoxic effects. Moreover, the 428 need for conjugation with radionuclides with extended half-lives and a long period between radiotracer 429 administration and imaging is not conducive to clinical translation. Our decision to use ¹⁸F-radiolabeled 430 FAPI was a strategic choice to address this issue as ¹⁸F is a scaleable radioisotope used in routine clinical 431 PET imaging (e.g. [¹⁸F]FDG imaging in oncology) (30) and would facilitate transition into the clinic in terms 432 of both productions and meeting the clinical demand.

433

434 One of the key challenges of FAP-targeted therapies is that the antigen is also expressed at low levels in 435 limited healthy tissues including bone marrow mesenchymal stem cells, muscle, and the pancreas (31,32). 436 From the ex vivo biodistribution analysis following [¹⁸F]AIF-FAPI-74 imaging, we were able to identify 437 organs that have endogenous FAP expression in our xenograft mouse model and the potential effect of 438 FAP CAR T cell therapy on these organs (Figure 6A). For example, the %ID/g in both the bone marrow and 439 the bone of the FAP CAR T cell-treated group was reduced compared to the NTD T cell-treated group. This 440 suggests that there is some FAP expression in both the bone marrow and the bone of NSG mice, and the 441 cells expressing FAP in these organs are affected by FAP CAR T cell therapy. Bone marrow suppression is 442 a reported outcome of FAP CAR T cell therapy in different mouse models (32,33), however, 443 immunohistochemical staining and flow cytometry studies showed differences in FAP expression in mouse 444 versus human bone marrow (unpublished). Furthermore, a human biodistribution study with [¹⁸F]AIF-445 FAPI-74 demonstrated low uptake in normal organs (15), providing support that FAP expression is limited 446 in healthy adult tissues. Regardless, the overall finding highlights the potential clinical utility of [¹⁸F]AIF-447 FAPI-74 in identifying patients who are likely to have an on-target/off-tumor toxicity in case of increased 448 FAP expression at an off-tumor site, for example in the case of a healing wound or unknown fibrotic 449 process. In addition to its potential use in the clinic, the tool may also be applied in pre-clinical settings to 450 aid in the development of CAR T cell clinical protocols, including in the assessment of scFv affinity and 451 different armoring strategies, to maximize the therapeutic window and minimize on-target/off-tumor 452 toxicity. In our model, other organs of concern such as the pancreas and muscle did not have significant 453 FAP expression that was affected by FAP CAR T cell therapy.

454

In this study, we demonstrated a clear correlation between [¹⁸F]AIF-FAPI-74 imaging and IHC of the FAP⁺
 tumors. For example, our PET imaging was able to pick out the uniform, homogenous expression of FAP
 in the I45 huFAP tumor (Supplemental Video S1) whereas the A549 tumor showed heterogeneous and

458 patchy foci of tracer uptake from the infiltrating fibroblasts (Supplemental Video S2). Such differential

459 pattern of uptake between the two tumors was also apparent in *ex vivo* IHC (Figure 2D and Figure 3C). 460 Correlating the [¹⁸F]AIF-FAPI-74 PET signal and FAP signal quantified by IHC following treatment with 461 either FAP CAR T cells or NTD control T cells, we observed a strong, positive relationship between the two 462 measurements (Figure S7). This highlights the potential of [¹⁸F]AIF-FAPI-74 imaging to complement 463 biopsy-based IHC as well as map out and monitor target expression following a therapeutic intervention. 464 While the tumor sizes were still measurable following CAR T cell therapy, they were smaller compared to 465 the non-transduced T cell-treated group (Figure 5B) and could have introduced a small, but possible 466 quantification bias (partial volume effect). In the future, using reconstruction parameters that can help 467 increase the effective resolution or applying appropriate correction methods could help minimize the bias 468 (34, 35).

469

470 While our data support that [¹⁸F]AIF-FAPI-74 PET is an ideal candidate for non-invasive characterization of 471 FAP expression and for monitoring of response to FAP CAR T cell therapy, future studies should focus on 472 evaluating whether the observed changes in FAP expression ultimately predict long-term therapeutic 473 success in terms of progression-free and overall survival and whether the degree of tracer uptake 474 corresponds to and is a strong predictor of response to FAP CAR T cell therapy. This would be important 475 given that FAP⁺ cells tend to regenerate over time following therapy (13), and long-term monitoring of 476 patients with [18F]AIF-FAPI-74 PET would help inform clinical decision-making (e.g. re-dosing or dose 477 optimization, change of therapy, etc.).

478

479 FAP CAR T cell therapy has the potential to be used in conjunction with other immunotherapies and 480 potentiate their use in the clinic given its unique ability to permeabilize dense tumor microenvironment 481 and tear down the physical barrier masking the tumor antigens (10). Therefore, imaging probes that can 482 untangle the efficacy of one therapy from another will be useful in guiding patient care. For example, FAP 483 CAR T cells have been paired with PD-1 blocking antibody and showed that the combination therapy 484 results in better tumor control and improved survival in a humanized model of malignant pleural 485 mesothelioma (36), a clinical indication where PD-1 blockade had previously failed to demonstrate a 486 strong therapeutic response (37). In such dual-therapy models, monitoring and re-assessing FAP 487 expression with a tool like [¹⁸F]AIF-FAPI-74 PET may be critical in understanding whether the therapy is 488 working as expected and also in identifying the ideal time to initiate the second therapy. PET imaging 489 approaches can help to separate the results from complex therapies and can offer complementary data 490 to the standard of care approaches such as IHC and serum biomarkers.

491

492 Although FAP is generally expressed at low levels in healthy tissues, its upregulation has been implicated 493 in a wide range of non-oncologic indications (38). For example, FAP-targeted CAR T cells have been shown 494 to specifically target activated cardiac fibroblasts and significantly reduce cardiac fibrosis to restore 495 cardiac function (39). Pulmonary fibrosis is another fibrotic condition characterized by high FAP 496 expression, and could also benefit from non-invasive characterization of FAP expression (40). Currently, 497 there are very few drugs approved for the treatment of fibrotic conditions (41). Although the 498 development of such drugs to treat fibrosis is a high priority, one potential limitation will be the ability to 499 distinguish "active fibrosis" from "scar". The former will likely be much more amenable to therapies such 500 as kinase inhibitors, drugs targeted to fibroblasts, or cytokine and growth factor inhibitors. Since FAP is 501 primarily expressed during active tissue remodeling (42), the ability to use FAPI imaging to both screen 502 for the most potentially treatable patients and then to follow the response to treatments could be 503 paradigm-changing. Furthermore, cardiotoxicity is a known complication of many cancer treatments, 504 including immunotherapies such as checkpoint inhibitors (43). Detection of activated cardiac fibroblasts 505 using FAPI imaging could help understand signs of immunotherapy-induced myocardial damage early in 506 the treatment course, prevent further cardiotoxicity, and guide clinical care (44,45). The molecular

- 507 imaging biomarker paradigm presented in this work aims to provide a better understanding of target
- 508 biology and heterogeneity, and thereby help tailor therapies to deliver personalized precision medicine 509
- to patients.

510 Disclosure of Potential Conflicts of Interest

- 511 SMA and EP report receiving research support for pre-clinical studies of FAP CAR T cells in solid tumors
- 512 from TMUNITY and both are co-founder of CAPSTAN Therapeutics Inc. and receive research funding from
- 513 the company for pre-clinical studies of FAP CAR T cells in fibrosis. CHJ: Royalties from Novartis. Scientific
- 514 advisor for AC Immune, Alaunos, BluesphereBio, Cabaletta, Capstan, Carisma, Cartography, Cellares,
- 515 Celldex, DeCART, Decheng, Poseida, Verismo, Viracta, and WIRB-Copernicus Group. MAS is a co-founder
- 516 of Vellum Biosciences related to PET imaging of genetic therapies. The other authors declare no potential
- 517 conflicts of interest.
- 518

519 Author Contributions

- 520 Conception and design: I. Lee, S. Albelda, E. Puré, M. Sellmyer
- 521 **Development of reagents and methodology**: I. Lee, E. Noguera-Ortega, Z. Xiao, L. Todd, K. Lohith, D.
- 522 Song, J. Scholler, C. June
- 523 Acquisition of data (provided animals, acquired and managed patients, provided facilities, etc.): I. Lee,
- 524 E. Noguera-Ortega, Z. Xiao, L. Todd, K. Lohith, M. Farwell, S. Albelda, E. Puré, M. Sellmyer

525 Analysis and interpretation of data (e.g., statistical analysis, biostatistics, computational analysis): I.

- 526 Lee, E. Noguera-Ortega, Z. Xiao
- 527 Writing, review, and/or revision of the manuscript: I. Lee wrote the draft of the manuscript, with all
- 528 authors, especially E. Noguera-Ortega, Z. Xiao, S. Albelda, E. Puré, and M. Sellmyer contributing to the 529 revision.
- 530 Administrative, technical, or material support (i.e., reporting or organizing data, constructing
- 531 databases): M. Sellmyer
- 532 Study supervision: M. Sellmyer
- 533

534 Acknowledgments

535 We thank members of the UPenn Human Immunology Core, the Small Animal Imaging Facility (Eric 536 Blankemeyer), and the Flow Cytometry and Cell Sorting Facility. We thank Sherly Mosessian, Frank Valla 537 (SOFIE Biosciences), and David Barrett (Tmunity) for their comments. Illustrations were created with

538 <u>Biorender.com</u>. MAS is supported by the National Institute of Health Office of the Director Early

539 Independence Award (DP5-OD26386), Burroughs Wellcome Fund Career Award for Medical Scientists. IKL 540 and this research was supported by Institute for Translational Medicine and Therapeutics (ITMAT). SMA

- and this research was supported by Institute for Translational Medicine and Therapeutics (ITMAT). SMA and EP are supported by P01 CA217805 from the National Cancer Institute. We also would like to
- 542 acknowledge the Kathleen M. Rotz Lung Cancer Research Fund for partial support of this study.

543 Figures



544 545

Figure 1. Structure of [¹⁸F]AIF-FAPI-74 and its uptake in FAP-expressing cells *in vitro*.

546 **(A)** Structure of FAPI-74 and radiolabeled [¹⁸F]AIF-FAPI-74. **(B)** 1x10⁶ I45 WT and human FAP-transduced 547 I45 cells (I45 huFAP) were incubated with [¹⁸F]AIF-FAPI-74 for 1 hour at 37°C in the presence or absence

547 I45 cells (I45 huFAP) were incubated with [18 F]AIF-FAPI-74 for 1 hour at 37°C in the presence or absence 548 of unlabeled FAPI (10µM). The *in vitro* uptake study demonstrated a greater than 100-fold increased

of unlabeled FAPI (10 μ M). The *in vitro* uptake study demonstrated a greater than 100-fold increased uptake of the tracer in I45 huFAP cells relative to WT and blocked controls. n=3, data points are mean

 $550 \pm$ SD. Uptake was measured as percent injected dose per gram (%ID/g) with a gamma counter. Groups

551 were compared using a two-way ANOVA with Tukey's multiple comparisons test. ****p<0.0001, ns = not

552 significant.



553 554

54 Figure 2. Imaging of FAP Expression in a I45 Mesothelioma Xenograft Model *In Vivo*

555 (A) Representative [¹⁸F]AIF-FAPI-74 PET images of 3 different NSG mice (M742, M743, M744 refer to 556 mouse number) xenografted with I45 WT (left side, blue ROI) and I45 huFAP mesothelioma tumor (right 557 side, red ROI) showed a selective uptake of the tracer in the FAP-expressing, I45 huFAP tumor. [18F]AIF-558 FAPI-74 PET/CT images were acquired 1 hour post-radiotracer administration. (B) For [¹⁸F]AIF-FAPI-74 PET 559 quantification, ROIs were drawn around I45 tumors and background muscle. The left panel shows the raw 560 tumor uptake in SUV_{mean} and SUV_{max}, and the right panel shows the tumor-to-muscle ratio calculated by 561 dividing the signal from the tumors by the signal from the muscle. I45 huFAP tumor demonstrated 7 to 8-562 fold higher tracer uptake relative to the WT tumor. n=10, data points are mean \pm SD. Groups were 563 compared using an unpaired t-test (two-tailed). ****p<0.0001. (C) Ex vivo biodistribution analysis performed following terminal [¹⁸F]AIF-FAPI-74 imaging (approximately 1.5 hours post-radiotracer 564 565 administration) showed 12 and 15-fold increased tracer retention in FAP-expressing huFAP tumor relative 566 to the WT tumor and background organs, respectively. n=6, data points are mean \pm SD. Groups were

- 567 compared using a one-way ANOVA with Tukey's multiple comparison test. ****p<0.0001, ns = not
- 568 significant. (D) Representative IHC images of A549 tumor sections stained with antibodies against FAP, α-
- 569 SMA, PDGFR α , and DAPI, demonstrate robust FAP expression in the I45 huFAP tumor. Scale = 100 μ m.



570 571

Figure 3. Imaging of Mouse Stromal FAP Expression in an A549 Lung Adenocarcinoma Xenograft Model

572 In Vivo

(A) Representative [¹⁸F]AIF-FAPI-74 PET images of 2 different NSG mice (M4216 and M4217 refer to mouse
 number) xenografted with A549 lung adenocarcinoma tumor (right side, pink ROI) 1 hour post-radiotracer
 administration demonstrated retention of [¹⁸F]AIF-FAPI-74 tracer in the tumor area. (B) [¹⁸F]AIF-FAPI-74

576 PET quantification, with the left panel showing the raw tumor uptake in SUV_{mean} and SUV_{max}, and the right

577 panel shows the tumor-to-muscle ratio. Target-to-background ratio demonstrated 4 (SUV_{mean}) to 6.5-fold

- 578 (SUV_{max}) higher uptake in the A549 tumor relative to muscle. n=8, data points are mean \pm SD. (C)
- 579 Representative IHC images of A549 tumor sections stained with antibodies against FAP, α -SMA, PDGFR α ,
- 580 and DAPI, demonstrate robust FAP expression in the tumor, validating PET imaging findings. Scale =
- 581 100μm.



582 Figure 4: *In Vitro* Characterization and Validation of FAP CAR T Cell Effector Function

583 (A) Schematic of pTRPE L2HG FAP CAR-T2A-mCherry backbone. CD3 and mCherry are separated by a T2A 584 cleavage site. (B) Primary human T cells were transduced with pTRPE L2HG FAP CAR-T2A-mCherry 585 lentivirus at MOI of 5 and transduction efficiency was assessed with flow cytometry using mCherry and 586 AF647-conjugated F(ab')₂ fragment. Transduced cells were sorted on mCherry expression and AF647 stain 587 for downstream assays. (C) Target-specific cytolytic activity of FAP CAR T cells were tested by co-588 incubating them with I45 WT and I45 huFAP target cells overnight. The assay demonstrated an Effector-589 to-Target ratio (E:T)-dependent killing of the target cells. Percent specific cytotoxicity was determined 590 using MTS assay. n=3, data points are mean \pm SD. Groups were compared using a two-way ANOVA with 591 Šídák's multiple comparisons test. ****p<0.0001, ns = not significant. (D) IFNγ and TNFα secretion from 592 effector FAP CAR T cells following an overnight exposure to target I45 cells. The level of cytokine secretion 593 was determined by ELISA. Data points are mean \pm SD and groups were compared using a two-way ANOVA 594 with Tukey's multiple comparisons test. ****p<0.0001.



596 Figure 5: Monitoring of Therapeutic Response to FAP CAR T Cell Therapy

595

597 (A) Schematic of experimental timeline. NSG immunodeficient mice were subcutaneously xenografted 598 with A549 tumor. The tumors were grown for 3 weeks, and all animals were imaged on small animal 599 PET/CT 1 hour following [¹⁸F]AIF-FAPI-74 administration to establish a baseline uptake. Animals were then 600 randomized to receive either 5x10⁶ CAR⁺ FAP CAR T cells or cell number-matched non-transduced control 601 (NTD) T cells via tail vein. The mice were imaged again with [18F]AIF-FAPI-74 2 weeks following T cell 602 injection for terminal PET imaging and downstream tissue processing. (B) Tumor volume data between 603 CAR T cell injection (Day 0) and follow-up [¹⁸F]AIF-FAPI-74 PET/CT scan (Day 14) demonstrated a 604 statistically significant decrease in tumor volume for the FAP CAR T cell-treated group relative to the NTD 605 control T cell-treated group. n=4 for NTD control T cell group, n=8 for FAP CAR T cell group. Data points 606 are mean \pm SD. Data for Day 14 between the two groups were compared using an unpaired t-test (two-607 tailed). **p=0.0011. (C) Representative [¹⁸F]AIF-FAPI-74 PET/CT images showed statistical differences in 608 tracer uptake between FAP CAR T cell-treated (right, M4917) and non-transduced (NTD) T cell-treated 609 (left, M4916) animals. (D) [¹⁸F]AIF-FAPI-74 PET quantification demonstrated a 2 (SUV_{mean}) to 3-fold 610 (SUV_{max}) reduction in target tumor-to-muscle uptake ratio for FAP CAR T cell-treated group relative to the 611 baseline scan. n=4 for NTD control T cell group, n=8 for FAP CAR T cell group. Data points are mean \pm SD. 612 Groups were compared using a one-way ANOVA with Tukey's multiple comparison test. *p=0.0151, 613 ****p<0.0001.



614 Figure 6: Tumor Measurement, *Ex Vivo* Biodistribution, and Tumor Analysis for Correlation with

615 Radiologic Findings

616 **(A)** *Ex vivo* biodistribution analysis following the terminal [¹⁸F]AIF-FAPI-74 PET/CT imaging time point on 617 Day 14 showed around 3-fold higher tracer retention in the NTD control T cell-treated tumor compared 618 to the FAP CAR T cell-treated tumor. Data points are mean \pm SD and groups were compared using a two-619 way ANOVA with Šídák's multiple comparisons test. **p=0.0065, ****p<0.0001, ns = not significant. **(B)**

- 620 Flow analysis of cell population in the A549 tumor treated with FAP CAR T cell vs. NTD control T cells
- 621 showed a higher percentage of total CD45⁺ in FAP CAR T cell-treated tumor. Groups were compared using
- a Mann-Whitney test. **p=0.0040. (C) Representative IHC images of A549 tumor sections stained with
- 623 antibodies against FAP, α -SMA, PDGFR α , and DAPI. A549 tumor harvested from animals treated with FAP
- 624 CAR T cells showed lack of FAP expression and patchy areas of apoptotic cells, whereas tumor harvested
- 625 from NTD-treated animals showed intact and robust expression of FAP, validating PET imaging findings.
- 626 Scale = 100μm.

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